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## Enzyme encapsulation in metal–organic frameworks for applications in catalysis

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Enzymes are natural catalysts which are highly selective and efficient. Given that enzymes have very intricate and delicate structures, they need to be stabilized and protected by a support material if they are to be used under challenging catalytic conditions. This highlight focuses on the use of metal–organic frameworks as supports for enzyme encapsulation and subsequent catalytic applications. *De novo* and post-synthetic methods of encapsulation are discussed and the relative catalytic activities of the enzyme@MOF composites *versus* free enzymes are highlighted.

### 1. Introduction

Throughout our existence, humans have looked to Nature and natural systems for inspiration in solving complex problems such as self-healing,<sup>1</sup> aerodynamics,<sup>2</sup> solar energy harvesting<sup>3</sup> and catalysis.<sup>4,5</sup> Biological processes have been subject to millions of years of evolutionary experimentation giving rise to structures and functions with remarkable efficacy.<sup>6</sup> One class of biomacromolecules of interest from a biomimetic<sup>7</sup> standpoint is enzymes – Nature's catalysts.<sup>8,9</sup> En-

zymes are linear sequences of amino acids that fold to give intricate structures with highly specific catalytically active sites. As a result, enzymes produce highly selective (regio-, stereo-, chemo-) products with accelerated reaction rates and high turnover numbers.<sup>10</sup> Given that enzymes are selective, efficient and environmentally benign catalysts, they have found application in a handful of large-scale processes such as the production of fine and pharmaceutical chemicals.<sup>11–13</sup> Advances in protein engineering, sequence analysis and computational modelling allow for the fine tuning of enzymes to control aspects such as substrate recognition, efficiency and the nature of the product formed.<sup>8,9</sup> The ability to make designer enzymes tailored for specific chemical transformations makes biocatalysis a very promising avenue for a variety of industrial processes.<sup>14</sup> The application of enzymes thus far however, has been limited, in part due to the lack of long-term stability and difficulties with recyclability and

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separation and transport to drive molecular solar fuels catalysts and the design of functional inorganic materials.

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metal–organic frameworks (MOFs) as adsorbents.

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recovery.<sup>15</sup> The immobilization of enzymes on solid supports is one possible solution for promoting the industrialization of enzymes as catalysts.<sup>15,16</sup> Immobilization can lead to increased enzyme stability, handling and recoverability-factors that in turn reduce cost. Solid supports that have been studied for enzyme immobilization include, but are not limited to, silicate glass,<sup>17,18</sup> graphene oxide,<sup>19</sup> carbon nanotubes,<sup>20</sup> nanoparticles,<sup>21</sup> mesoporous silica,<sup>22</sup> macroporous polymeric beads such as Eupergit C® (ref. 23, 24) and metal-organic frameworks (MOFs).<sup>25–27</sup>

Metal-organic frameworks offer many intriguing properties that make them of interest for enzyme immobilization.<sup>25–28</sup> Given that MOFs are composed of both inorganic and organic components, several kinds of interactions between the MOF support and enzyme are possible. Among

them are hydrogen bonding, including salt-bridge formation; other van der Waals forces, including dispersion forces; and covalent and/or coordinative bonding. Dispersion forces, while typically negligible for small molecules, can be large (and even predominant) for macromolecules, where their magnitude scales with the number of polarizable electrons. Since the strength of dispersion interactions varies strongly with distance, appropriate size matching of MOF pores to enzyme axes should enhance these interactions. The crystalline and ordered nature of MOFs allows for uniform loading, less leaching and an understanding of the local environment around the immobilized enzyme.<sup>25,29</sup> The structures of MOFs are highly tunable such that surface area as well as pore size, shape and volume can be optimized for the immobilization and/or encapsulation of specific enzymes. Lastly, MOFs can



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*His research interest is related to functional porous materials for gas storage, separations, catalysis, and enzyme immobilization.*

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be designed to be robust under harsh thermal, mechanical and chemical conditions<sup>30</sup> which is important for immobilization and subsequent protection of enzymes to be used under challenging catalytic conditions. While enzymes can be immobilized on the surface of MOFs,<sup>31–39</sup> this highlight will focus on examples of enzymes immobilized inside MOFs (*i.e.* encapsulation) with an emphasis on catalytic applications. The most obvious potential benefit of encapsulation is physical inhibition of enzyme denaturation (*i.e.* unfolding or changing of shape) in response, for example, to heating, dehydration, or changes in solution ionic strength. With good size matching between enzymes and MOF pores, encapsulation can also serve to prevent enzyme deactivation *via* aggregation. Although not yet widely explored, appropriately tailored MOF pores may provide local buffering or otherwise optimize the enzyme's microenvironment. The synthetic methods used to encapsulate enzymes and important design rules for MOF-based bioreactors will be discussed.

## 2. Enzyme immobilization in MOFs

One can imagine that biomacromolecules such as enzymes may be encapsulated within MOFs *via* two general strategies: by assembling the MOF around the enzyme (which we term *de novo* encapsulation) or by introducing the enzyme into the pre-existing MOF (which we term post-synthetic encapsulation). Each route manifests implications regarding preserving enzyme activity, efficiency and stability while at the same time dictating the conditions that may be used to prepare the supporting framework. In addition to considerations regarding the method of encapsulation, in systems prepared for catalytic applications, it is important to consider the effect that the chosen framework may have on factors such as substrate diffusion and/or selectivity. Coefficients for molecular diffusion through MOFs are typically much smaller than for diffusion through aqueous solutions. Thus, even MOF crystallite size can be important, as diffusion times increase as the square of the distance travelled. Clearly, in order to maximize catalyst performance, a delicate balance of these factors must be considered when selecting or tailoring supported catalytic systems for specific applications.

We begin with examples of *de novo* encapsulation methods *via* processes known as coprecipitation and biomimetalization, two related strategies each with its own advantages. Subsequently, we discuss post-synthetic methods of enzyme encapsulation using both channel- and cage-type MOFs as examples (Fig. 1).

### 2.1 Enzyme incorporation *de novo*

In general, *de novo* approaches revolve around combining the organic and inorganic building blocks of the framework together with the target enzyme under conditions that favor both framework formation and preserve the tertiary structure of the active enzyme. Most MOFs present channels and/or apertures that are smaller than the size of the folded enzyme (see section 2.2) – thus the need to assemble the MOF around

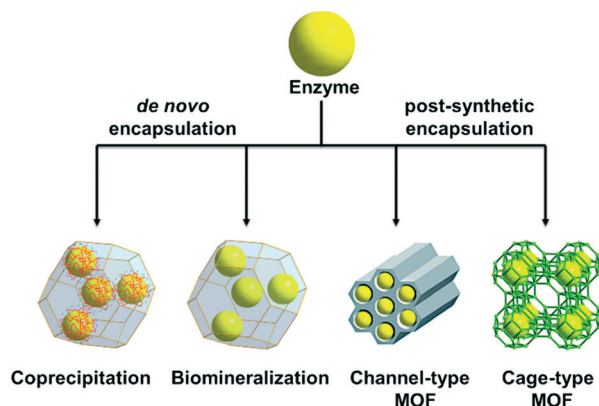


Fig. 1 Methods used to encapsulate enzymes in MOFs.

the enzyme. Underscoring the novelty of this burgeoning field, little (non-MOF) literature precedent exists for this approach; however, within the MOF field several groups have reported compelling examples of its applicability.

**2.1.1 Coprecipitation.** Described as a coprecipitation method, Lyu and coworkers have reported embedding cytochrome *c* (Cyt *c*) in a zeolitic imidazolate framework (ZIF-8) through the reaction of zinc nitrate hexahydrate, 2-methylimidazole, Cyt *c* and polyvinylpyrrolidone (PVP) in methanol (Fig. 2).<sup>40</sup> Here, the presence of PVP was required to stabilize and disperse Cyt *c* in methanol. Transmission electron microscopy (TEM) confirmed the formation of ZIF-8 rhombic dodecahedron crystals, while calcination was carried out to remove protein molecules from the scaffold revealing the formation of small cavities corresponding to the

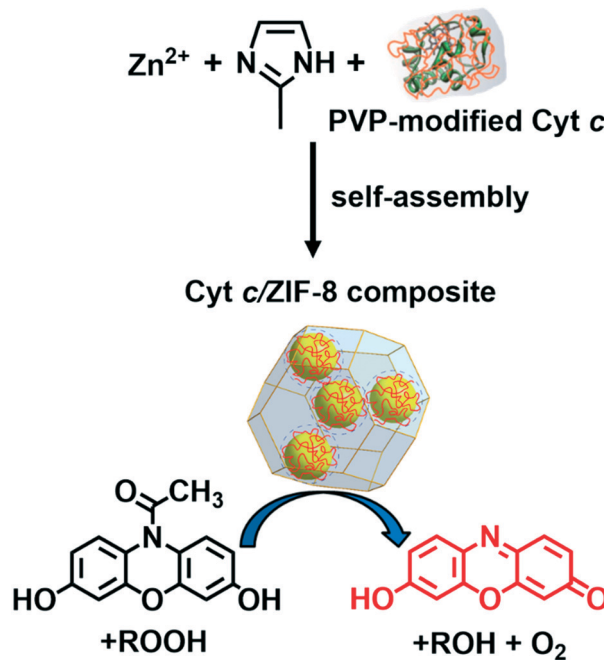


Fig. 2 Encapsulation of Cyt *c* in ZIF-8 by coprecipitation for the detection of organic peroxides.



size of Cyt *c* molecules and their aggregates. These composites were found to exhibit 10-fold greater catalytic activity when compared to the enzyme in solution. In a representative study, the authors report that the peroxidase activity of the Cyt *c*@ZIF-8 composite in the presence of H<sub>2</sub>O<sub>2</sub> (among other peroxides) and *N*-acetyl-3,7-dihydroxyphenoxazine (Amplex Red) substrates yields the oxidation product of Amplex Red, resorufin, a fluorescent reporter. In this ensemble, the fluorescence of resorufin was measured after a 2 minute incubation in tris-HCl buffer (50 mM, pH 7.4) at room temperature. Notably, the peroxide detection limit with this system is reported to be 3 nM, with the limit being defined as a signal-to-noise ratio of 3. Free Cyt *c* yields a considerably slower reaction rate under identical conditions and no detectable fluorescence signal. The utility of this coprecipitation approach was further realized through incorporation of horseradish peroxidase and lipase into ZIF-8 and ZIF-10.

Although coprecipitation provides a direct and relatively facile route to the formation of these biocomposite materials, employing synthetic conditions that require the target enzyme to be independently stabilized against denaturation is a complicating factor. ZIF-8 is a framework with relatively small apertures (*ca.* 0.35 nm static diameter, dynamically expandable to about 0.5 nm). The consequences are slow substrate diffusion (compared to aqueous solution),<sup>41</sup> thereby potentially limiting the catalytic activity of encapsulated enzymes, as well through exclusion of candidate substrates or co-reactants larger than *ca.* 0.5 nm. Nevertheless, the ZIF family of frameworks is a logical foundation for the coprecipitation method owing to the mild conditions that can be used for synthesis, the synthetic ease of linker modification to enhance framework-enzyme interactions, and the resistance of many ZIFs to degradation by water.<sup>41–43</sup>

To combat enzyme denaturation Shieh *et al.* pursued *de novo* enzyme encapsulation (catalase in ZIF-90; Fig. 3) in aqueous solution.<sup>44</sup> Catalase (CAT), an industrially important enzyme employed for wastewater remediation, must be shielded in a matrix to prevent interaction with protease; an enzyme typically used up-stream of catalase. Although the peroxidase activity of catalase is retained, the report from

Shieh, *et al.* illustrates some of the complications of *de novo* enzyme encapsulation by comparing composites formed in water *versus* ethanol. Perhaps unsurprisingly, using the conventional ethanol-based ZIF-90 preparation method yields a CAT@ZIF-90 composite that is catalytically inactive. In contrast, the aqueous sample is catalytically active, yielding an observed rate constant ( $k_{\text{obs}}$ ) of 0.0268 s<sup>-1</sup>. Further highlighting the degree of optimization complexity in these types of systems, Shieh and coworkers report that the rate constant with this composite is lower than that with free CAT in solution ( $k_{\text{obs}} = 0.897 \text{ s}^{-1}$ ), implying a non-ideal interface between ZIF-90 and catalase, some degree of catalase denaturation, and/or mass transport limitations.

In an attempt to impart multifunctionality to these new materials, Wu and coworkers reported the successful encapsulation of two different enzymes, glucose oxidase (GOx) and horseradish peroxidase (HRP) in ZIF-8 *via* coprecipitation.<sup>45</sup> Confocal laser scanning microscopy of composites containing fluorescein isothiocyanate (FITC) labelled GOx and HRP confirmed the presence of both enzymes within the crystal. In a display of intricate chemical cooperativity, catalytic efficiency of this composite was measured by indirectly detecting glucose through the formation of negatively charged 2,2'-azino-bis(3-ethylbenzothiazoline-6-sulphonic acid) (ABTS<sup>-</sup>) which has an electronic absorption band centered at 415 nm. In this scheme, GOx converts glucose into gluconic acid while concomitantly generating H<sub>2</sub>O<sub>2</sub> that is then used as a substrate by HRP to oxidize ABTS<sup>2-</sup> to ABTS<sup>-</sup>. Notably, this method led to a fair detection limit of 0.5 μM. Denaturation and degradation of this pair of enzymes is thwarted by the rigid ZIF-8 framework, which protects the encapsulated biomacromolecules from digesting enzymes and from chelating compounds, as illustrated experimentally by exposure of the composite to dissolved ethylenediaminetetraacetic acid. As expected, this composite also exhibits improved thermal stability *versus* the enzyme in solution.

**2.1.2 Biomimetalization.** Drawing inspiration from natural processes, Liang *et al.* have shown that enzymes (among other biomacromolecules) under physiologically relevant conditions can facilitate the formation of MOF coatings by allowing for the concentration of framework building blocks and by initiating crystallization (Fig. 4).<sup>47</sup> This process, reminiscent of biomineralization (a self-assembly process in Nature whereby characteristically complicated molecular architectures that provide structural support for soft tissue along with exoskeletal protection are generated), controls the morphology of the resulting crystal (as observed by SEM imaging) while preserving porosity. As in coprecipitation, this process encapsulates target biomacromolecules and preserves bioactivity by imparting a high degree of biological, thermal and chemical stability. In addition to thoroughly characterizing ZIF-8 composites, Liang and coworkers catalogued this behavior in a variety of other MOFs (HKUST-1, Eu/Tb-BDC and MIL-88A) by encapsulating bovine serum albumin. Impressively, biomimetic mineralization of ZIF-8 was observed with a myriad of enzymes, including but not limited to ovalbumin,

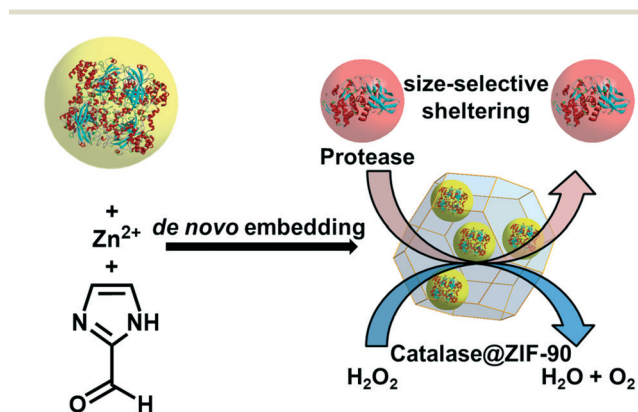


Fig. 3 *De novo* encapsulation of catalase in ZIF-90.

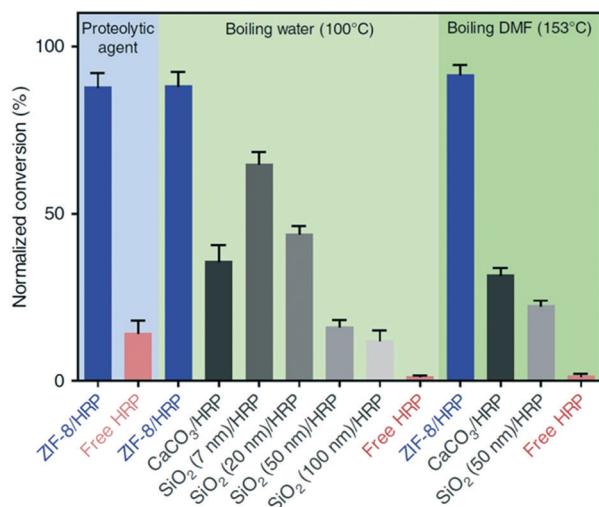


Fig. 4 Stability of horseradish peroxidase (HRP) encapsulated in ZIF-8 via biomineralization compared to other supports under varying conditions. Reproduced from ref. 46.

ribonuclease A, human serum albumin, lipase, insulin, horseradish peroxidase and urease. Further broadening the scope for application of these hybrid materials, it was demonstrated that varying the pH (from 7.4 to 6) around the ZIF-8 framework resulted in liberation of the encapsulated biomacromolecule with the liberated enzyme still displaying biological activity.

A direct comparison of composite urease@ZIF-8 prepared by coprecipitation (carried out in the presence of PVP in aqueous solution) and by biomimetic mineralization yielded similar encapsulation efficiencies (as determined by the amount of FITC labelled urease incorporated into the final material). Notably, the coprecipitation method resulted in smaller crystal sizes (120 nm *versus* 500 nm) resulting in an increased rate of enzymatic reaction, while the composites prepared by biomineralization exhibited enhanced stability over a larger breadth of temperatures.<sup>47,48</sup>

Although viable as strategies for embedding biomacromolecules such as enzymes in MOFs, coprecipitation and biomimetic mineralization are also susceptible to complications. Namely, for both methods, reaction conditions must be chosen such that framework formation is possible while preserving the activity and integrity of the target enzyme. This narrows the scope of reaction media largely to aqueous solutions, a synthetic condition not common for MOF synthesis.<sup>49</sup> Additionally, controlling biocomposite crystal size when employing these methodologies is challenging, resulting in materials that vary in catalytic activity.

One hybrid *in situ* encapsulation approach recently reported involves the formation of MIL-88A(Fe) hollow spheres *via* in-droplet microfluidics. These hollow spheres were used to encapsulate glycerol dehydrogenase, horseradish peroxidase and acetylcholinase.<sup>50</sup> Conversely, another hybrid approach involves the formation of MOF particles around a pre-formed microcapsule where an emulsion

containing *Candida antarctica lipase B* (CALB) was stabilized with UiO-66 nanoparticles and the capsule's core was further stabilized against degradation *via* growth of a ZIF-8 shell.<sup>51</sup> These methods, although more complicated than the strictly *de novo* enzyme encapsulation methods, allow for a greater degree of composite complexity while still preserving enzyme activity.

## 2.2 Post-synthetic enzyme incorporation

Enzymes can also be encapsulated in MOFs post-synthetically. This method typically involves soaking MOF crystals in a solution of the desired enzyme for anywhere from minutes to days at room or slightly elevated temperatures (*e.g.*, 37 °C) depending on the system. The enzymes to be immobilized are often dissolved in water or a buffer solution at physiological pH (~7.4). To identify the optimal solution for post-synthetic enzyme encapsulation, it is important not only to consider the pH at which both the enzyme and MOF are stable but also the chemical identity of the buffer components. For example, many MOFs are not stable in phosphate buffer solutions even though the pH of these buffers is in the optimal physiological range.<sup>30</sup> Post-synthetic enzyme encapsulation for catalytic applications has been demonstrated using both cage-type and channel-type MOFs and examples of each will be discussed below.

**2.2.1 Cage-type metal-organic frameworks.** Cage-type MOFs are those that contain pores that are larger than the aperture (window) through which the pore is accessible. Enzyme immobilization in cage-type MOFs can be thought of as a 'ship-in-a-bottle' approach where the enzyme fits in the cage (pore) of the MOF but does not easily fit through the apertures or windows of the framework used to access the pore. In some cases, the enzyme will fit through the apertures based on a size match between the shortest enzyme axis and the aperture of the MOF whereas in other examples the enzyme must undergo conformational changes to squeeze through the apertures. In the latter case, one risks enzyme deactivation if the conformational changes affect the active site and are not reversible.

The first example of enzyme encapsulation in a cage-type MOF was presented by Ma and coworkers where microperoxidase-11 (MP-11, 3.3 × 1.7 × 1.1 nm) was encapsulated in a Tb-based MOF (Tb-mesoMOF) with cages 3.9 and 4.7 nm in diameter and apertures of 1.3 and 1.7 nm, respectively (Fig. 5).<sup>52</sup> In this example the shortest axis of the enzyme is small enough to allow enzyme diffusion into both cages while leaving the 0.9 nm micropores throughout the framework unoccupied to permit subsequent infiltration of the composite by substrate molecules. The peroxidase activity (oxidation of 3,5-di-*t*-butyl-catechol) and subsequent stability of the encapsulated MP-11 enzyme was compared to the free enzyme in HEPES buffer solution and also to MP-11 immobilized on the mesoporous silica support, MCM-41. Although the initial rate of catalytic oxidation was found to be faster in the free enzyme (8.93 × 10<sup>-4</sup> mM s<sup>-1</sup>) compared to

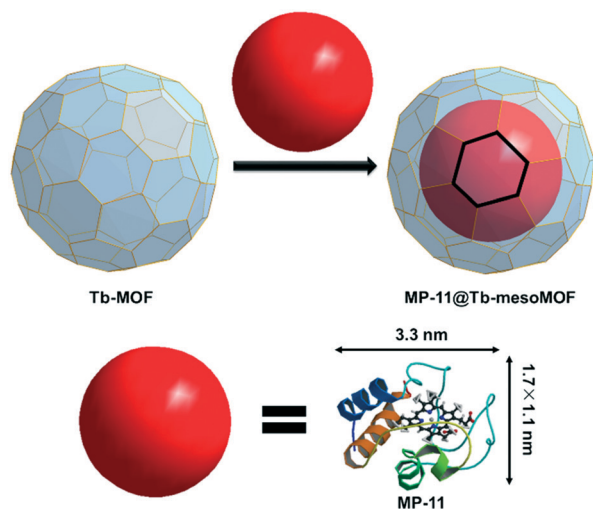


Fig. 5 Encapsulation of MP-11 in Tb-mesoMOF.

that immobilized in Tb-mesoMOF ( $7.58 \times 10^{-5} \text{ mM s}^{-1}$ ), the conversion after 25 hours was higher with the MOF composite (48.7%) than with the free enzyme (12.3%). While the silica and MOF composites showed similar initial reaction rates, the MOF-based bioreactor was shown to withstand 6 cycles of catalysis with negligible effect on the initial reaction rate whereas the MCM-41 composite showed a 60% decrease in the initial rate between the first and second reaction cycle. The superior recyclability of the MOF composite material was attributed to strong interactions between the hydrophobic MOF cages and the enzyme<sup>53</sup> compared to the weak interactions with MCM-41 which led to detectable enzyme leaching. An alternative explanation for the observation of leaching from MCM-41 *versus* an absence with Tb-mesoMOF is simply that the apertures of Tb-mesoMOF are too small to permit escape of the enzyme (but those for MCM-41 are not). That enzyme leaching is not observed with Tb-mesoMOF points to the stability of the MOF crystal in the reaction environment and also to the absence of defects of sufficient size to permit enzyme escape.

Ma and coworkers also immobilized myoglobin (Mb,  $2.1 \times 3.5 \times 4.4 \text{ nm}$ )<sup>54</sup> and cytochrome *c* (Cyt *c*,  $2.6 \times 3.2 \times 3.3 \text{ nm}$ )<sup>55</sup> in Tb-mesoMOF. In these examples the enzymes must undergo conformational changes to enter the cages of the MOF through the 1.3 and 1.7 nm apertures. In the case of Mb, the peroxidase activity of the enzyme was retained after encapsulation, albeit with a slower initial reaction rate ( $8.33 \times 10^{-6} \text{ mM s}^{-1}$ ) than that of the free enzyme ( $3.27 \times 10^{-4} \text{ mM s}^{-1}$ ). The Mb@Tb-mesoMOF was shown to retain catalytic activity over 15 cycles however, compared to Mb immobilized on the mesoporous silica support, SBA-15, which showed a 40% decrease in reaction rate after the first cycle. It is important to note that the size of the unoccupied channels (0.9 nm) in the enzyme@Tb-mesoMOF composites dictates the size of the substrate that can access the enzyme. For example, no peroxidase activity was observed using Mb@Tb-mesoMOF with 2,2'-azinobis(3-ethyl-benzthiazoline)-6-sulfonate (ABTS,  $1.0 \times 1.7$

nm) as a substrate whereas oxidation of 1,2,3-trihydroxybenzene (THB,  $0.57 \times 0.58 \text{ nm}$ ) was observed.<sup>54</sup> While not discussed in the Mb@Tb-mesoMOF work, the channel size should also be exploitable to prevent inhibitors or denaturants from accessing the enzyme.

The design and construction of cage-type MOFs with larger pores was undertaken by Zhou *et al.* to give MOFs with fewer size limitations for enzyme encapsulation.<sup>56</sup> PCN-333 has cages of 1.1, 3.4 and 5.5 nm in diameter with apertures of 2.6 and 3.0 nm in size. It was found that when encapsulating larger enzymes in PCN-333(Al) such as horseradish peroxidase (HRP,  $4.0 \times 4.4 \text{ nm} \times 6.8 \text{ nm}$ ) and Cyt *c*, the loading corresponds to encapsulation of 1 enzyme per cage, whereas with smaller enzymes such as MP-11, the loading corresponds to multiple enzymes incorporated per cage. In each case, the encapsulated enzyme demonstrates higher stability compared to the free enzyme, but lower initial reaction rates for oxidation of *o*-phenylenediamine (HRP) or ABTS (Cyt *c*, MP-11). The low initial reaction rates may be attributed to restricted diffusion of reactants and products and/or low enzyme accessibility in the cage-type structure. In order to overcome problems with reactant and product diffusion, Zhou and coworkers constructed PCN-888, an Al-MOF with cages of 2.0, 5.0 and 6.2 nm in diameter and apertures of 2.5 and 3.6 nm in size.<sup>57</sup> PCN-888 was used to selectively encapsulate glucose oxidase (GOx,  $6.0 \times 5.2 \times 7.7 \text{ nm}$ ) in the largest cage and HRP in the medium sized cage to give a tandem bioreactor with the smallest cages being unoccupied by enzymes, and therefore available for reactant and product transport (Fig. 6). In addition, the encapsulated enzymes were shown to be more stable than the free enzymes at slightly elevated temperature (37 °C) in the presence of trypsin. Although the initial reaction rate for the encapsulated enzyme is much closer to that of the free enzyme (compared to other examples of enzymes encapsulated in cage-type MOFs), the reaction rate is still slower than that found with the free enzyme.

**2.2.2 Channel-type metal-organic frameworks.** Channel-type MOFs are those that contain pores with some dimensions equal to the aperture dimensions through which the

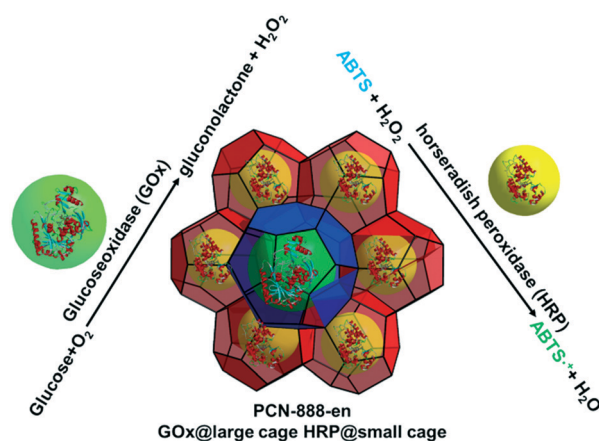


Fig. 6 Encapsulation of GOx and HRP in PCN-888 for tandem catalysis.



pore is accessible. Like cage-type MOFs, channel-type MOFs can have one single-sized channel, or multiple channels with different dimensions and geometries. In either case, depending on the framework topology, the channels can be accessible through windows present between the channels or only accessible from the two ends of the channels if the channel walls are dense with no (or limited) windows. The first example of an enzyme encapsulated in a channel-type MOF was shown by Pisklak, *et al.* where MP-11 was immobilized in a Cu-based MOF.<sup>58</sup> In this example the enzyme was shown to retain peroxidase activity and the Cu-based MOF demonstrated less enzyme leaching than a conventional mesoporous benzene silica (MBS) support. In a proof-of-concept study, Yaghi, Stoddart and coworkers synthesized a channel-type MOF, IRMOF-74-XI, with the largest apertures for any channel-type MOF reported at the time – 9.8 nm in diameter.<sup>59</sup> As part of this study on isorecticular expansion of MOF apertures/channels, green fluorescent protein (GFP, 3.4 nm diameter and 4.5 nm length) was encapsulated in the channels of IRMOF-74-IX (a MOF with apertures slightly smaller than IRMOF-74-XI) without having to undergo changes in conformation (Fig. 7).

The ideal MOF-based bioreactor should encapsulate and protect the desired enzyme but also allow for relatively unimpeded diffusive transport of reactants and products to and from the encapsulated enzyme, even when the enzyme is sited deep within the MOF. Hierarchical channel-type MOFs with windows between the channels are promising in this regard since large channels can be designed to fit the desired enzyme while small channels can remain unoccupied by enzymes and thus available for diffusive transport of small molecules. Windows between the channels can allow reactants access to the encapsulated enzyme in the larger neighbouring channels. We first demonstrated this concept using the hierarchical MOF, NU-1000, and the enzyme, cutinase.<sup>60</sup>

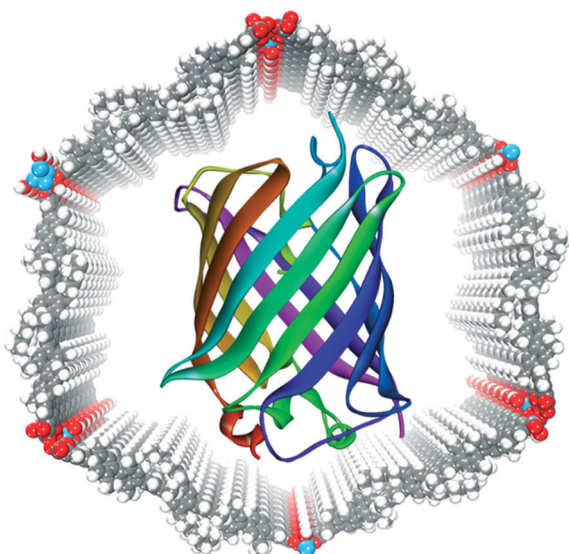


Fig. 7 Encapsulation of GFP in IRMOF-74-IX.

NU-1000 has triangular channels with an edge length of 0.9 nm and hexagonal channels which are 3.1 nm in diameter<sup>61</sup> meaning that cutinase (smallest axis is 3.0 nm) can be encapsulated in the larger pores while leaving the smaller pores open for delivery of reactants and release of products. Although cutinase loading in NU-1000 is not as high as in PCN-600 (a MOF with channels of only one size), experiments showed that more than 90% of the enzymes loaded in NU-1000 are accessible while only 6% of those in PCN-600 can be accessed. These findings highlight the importance of a hierarchical structure where smaller, enzyme-free channels enable molecular species, including solvent, to access the MOF interior, while windows between the smaller and larger channels permit molecules to reach enzymes throughout the MOF.

Using the same strategy, organophosphorus acid anhydrolase (OPAA, small axis is 4.4 nm) was encapsulated in PCN-128y, a MOF with hierarchical structure and larger hexagonal channels (4.4 nm) than NU-1000 to accommodate the larger enzyme.<sup>62</sup> The encapsulated OPAA enzyme was found to be more stable than the free enzyme, retain catalytic activity at temperatures up to 70 °C and after being dried and stored at room temperature for 3 days. Although the MOF was successful in stabilizing the OPAA enzyme, the initial rate of reaction for the hydrolysis of soman ( $56\text{--}75 \mu\text{mol min}^{-1} \text{mg}^{-1}$ ) was not as high as that found using the free enzyme ( $305 \mu\text{mol min}^{-1} \text{mg}^{-1}$ ). To enhance the reaction rate, NU-1003, a MOF with hierarchical structure containing 4.4 nm hexagonal channels, 1.7 nm triangular channels and windows between the channels of  $1.2 \times 1.3 \text{ nm}$  was designed to help promote molecular (reactant, product, solvent) transport and enzyme accessibility (Fig. 8).<sup>63</sup> In addition, the size of NU-1003 was controlled to give average MOF crystallites as particles ranging from 10  $\mu\text{m}$  down to 300 nm to further enhance diffusion. By capitalizing on these design concepts, we obtained a thus far rare

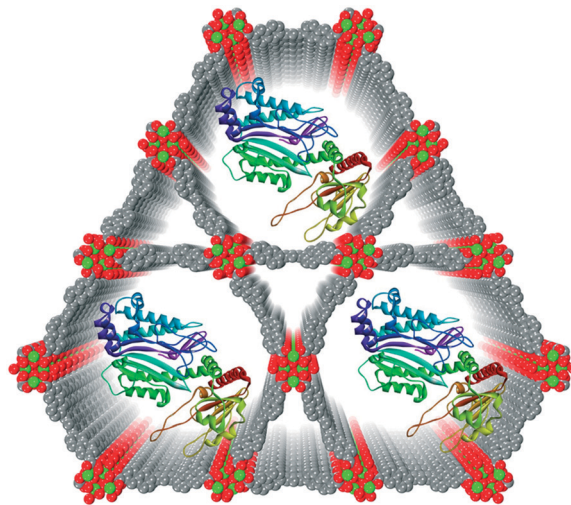


Fig. 8 Representation of encapsulation of organophosphorus acid anhydrolase (OPAA) in the hierarchical channel-type Zr-MOF, NU-1003.

example of a MOF-enzyme composite for which the initial rate of the catalyzed reaction is faster than that obtained with the free enzyme. Thus, the encapsulated enzyme OPAA was not only protected but also showed an initial reaction rate of  $960 \mu\text{mol min}^{-1} \text{mg}^{-1}$  for soman hydrolysis that is more than 3 times faster than that of the free enzyme (*i.e.*, detergent-stabilized enzyme in buffered aqueous solution).

### 3. Summary and outlook

As supports for stabilizing enzymes against environmental and incidental degradation, MOFs are an attractive target owing to their well-documented chemical and thermal stability. In addition, the immense library of known frameworks and the characterization of their respective properties and inherent stabilities paired with high porosity lends this class of materials to the formation of enzyme@MOF composites. Stabilizing enzymes against denaturation, while preserving native conformations of the biomacromolecule becomes especially important when encapsulating enzymes for specific catalytic purposes. The examples outlined here illustrate that enzyme@MOF composites can be effective at preserving enzyme activity while enforcing a greater degree of stability under catalytically relevant, but distinctly abiotic, conditions. Apart from a few examples, initial reaction rates for enzyme@MOF composites are not competitive with those of the free enzymes – but much has been learned about different encapsulation strategies and some design rules now exist for preparing enzyme@MOF composites that not only protect the encapsulated enzyme but also promote diffusion of reactants and products. It should be noted that the examples discussed throughout this highlight are based on the findings presented by different authors – in some cases the low initial reaction rates for enzyme@MOF composites compared to free enzymes may be a result of reactants/products not fitting through MOF apertures. In these instances, only enzymes immobilized on the surface of the MOFs may be active while all enzymes loaded into the framework may be assumed to be active. Thus, it is important to consider not only the size of the enzymes being encapsulated but also the size of the reactants/products of the reaction of interest.

Current research efforts into enzyme@MOF composites that were not discussed in this highlight include encapsulating enzymes into materials for chemical sensing.<sup>64–69</sup> One can imagine designing hybrid composites, where complex systems that first initiate a catalytic transformation are combined with a sensing component that detects specific catalytic products leading to direct measures of catalytic efficiency, reaction progress, or substrate concentration. One additionally important direction for the study of composites prepared from cage- and channel-type MOFs includes encapsulating enzymes into MOFs that feature high densities of missing-linker and/or missing-node type defects. This would allow for enzyme@MOF composites that were previously only attainable *via de novo* routes to be attainable post-synthetically.<sup>70</sup>

Significant progress has been made since the first example of enzyme encapsulation in a MOF was reported a decade ago. Hypothesis-driven research has led to enzyme@MOF composites that display initial catalytic reaction rates higher than those engendered by free enzymes. By using the set of design rules now established, together with others that await discovery, an expansive library of new functional composites should be designable and experimentally obtainable, perhaps contributing to the next wave of applied biocatalysis.

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